Biosignals and Systems

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Frequency Transformations Probing a Signal

• Complex signals such as the EEG signal shown previously could be analyzed by probing with reference signals

• Crosscorrelation provides a mechanism for finding out if sinusoids are embedded in a complicated signal.

 For example, we could crosscorrelate the EEG signal with sinusoids having frequencies we think may be embedded in the signal.

 If the crosscorrelation function shows a high value at some time shift (r), that would suggest the presence of our sinusoid, or other reference signal, at that time shift (or, equivalently, at that phase shift).





Probing with Sinusoids











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- Thus, the sinusoidal components of a signal are also the frequency components of a signal; that is, the spectral characteristics of the signal or just "spectrum."
- A complete description of a waveform's frequency characteristics consists of two plots: - a plot of the components' magnitude verses frequency
 - a plot of the components' phase verses frequency.



Symmetry						
Some waveforms are symmetrical or anti- symmetrical about $t = 0$, so that one or the other of the components, a_n or b_n will be zero.						
Table 3-1 Functi	Table 3-1 Function Symmetries					
Fu N	nction Name	Symmetry	Coefficient Values			
Ev	en	x(t) = x(-t)	$b_n = 0$			
Od	ld	x(t) = -x(-t)	$a_n = 0$			
Ha	alf-wave	x(t) = x(T - t)	$a_n = b_n = 0$; for n even			
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Example 3-2 Find the Fourier Transform of the triangle waveform defined below. Find the first four Fourier Transform components.

$$x(t) = \begin{cases} t & 0 < t \le 5\\ 0 & 5 < t \le 1.0 \end{cases}$$
Solution. Find the cosine (a_n) and sine (b_n) coefficients. Then convert to magnitude (C_n) and phase (θ_n) if desired.
To find b_n

$$b_n = \frac{2}{T} \int_0^T x(t) \sin(2\pi i t_1 t) dt = 2 \int_0^1 t \sin(2\pi i t) dt$$

$$= \frac{1}{2\pi^2 n^2} [\sin(2\pi i t) - 2\pi i t \cos(2\pi i t)]_0^5$$

$$= \frac{1}{2\pi^2 n^2} [\sin(\pi i) - \pi i \cos(\pi i t)] = \frac{-1}{2\pi i} (\cos(\pi i t))$$

$$= \frac{1}{2\pi}, \quad \frac{-1}{4\pi}, \quad \frac{1}{6\pi}, \quad \frac{-1}{8\pi} = .159, \quad -.080, \quad .053, \quad -.040$$







Fourier Series **Complex Representation** Euler's identity allows us to describe the sine and cosine functions in terms of imaginary exponentials $\cos(2\pi n f_1 t) = \frac{1}{2} (e^{-j2\pi n f_1 t} + e^{-j2\pi n f_1 t})$ and $\sin(2\pi n_{1}t) = \frac{1}{i^{2}} \left(e^{-j2\pi n_{1}t} - e^{-j2\pi n_{1}t} \right)$ Using the complex representation of a sinusoid, the Fourier Transformation correlation equations can be written as a single equation: $C_n = \frac{1}{T} \int_{-\infty}^{T} x(t) e^{-j2\pi n f_1 t} dt$ n = 0.1.2.3...where: $C_n = \frac{a_n - jb_n}{2}$ 19

Transform













- A digitized waveform must necessarily be truncated to the length of the memory storage array, a process described as "windowing."
- The windowing process can be thought of as multiplying the data by some window shape.
- If the waveform is simply truncated and no further shaping is performed on the resultant windowed waveform (as is often the case),
 then the window shape is rectangular.
- The data length will largely determine spectral resolution

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Power Spectrum (continued)

 In the direct approach, the Power Spectrum is calculated as the magnitude squared of the Fourier Transform of the waveform of interest:

 $PS(f) = |X(f)|^2$

The Power Spectrum does not contain phase information

so the Power Spectrum is not a bilateral transformation it is not possible to reconstruct the signal from the Power Spectrum.

• Since the Power Spectrum does not contain phase information, it is applied in situations where phase is not considered useful.

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Spectral Averaging

- Just as time signals can be averaged, Power Spectra can be averaged.
- Even if only one signal is available, isolated segments of the data can be used.
- The Power Spectra determined from each segment is averaged to produce a spectrum that better represents the broad, or "global," features of the spectrum.
- This approach is popular when the available waveform is only a sample of a longer signal and spectral analysis can only estimate the real spectrum.
- When the Power Spectrum is based on a direct application of the Fourier Transform followed by averaging, it is commonly referred to as an average "periodogram."













Frequency Methods MATLAB Implementation

The basic Fourier Transform routine is implemented as:

Xf = fft(x,n)% Calculate the Fourier Transform

where x is the input waveform and Xf is a complex vector providing the sinusoidal coefficients.

The argument n is optional and is used to modify the length of data analyzed:

if n is less than the length of x, then the analysis is performed over the first n points.

If n is greater than the length of x, then the signal is padded with trailing zeros to equal n. The fft routine uses the "Fast Fourier Transform" algorithm

that requires the data length to be a power of two: other data lengths will require longer calculation times. ³⁹



Example 3-6 Construct the waveform used in Example 3-1 and determine the Fourier Transform using both the MATLAB fft routine and a direct implementation of the defining equations (Eqs. 3-8). Solution: The MATLAB fft routine does no scaling so its output should be multiplied by 2/N, where N is the number of points to get the correct coefficients in rms value. To get the peak-to-neak values, the output will have to be further scaled by dividing by 0.707. N = 256% Data length

t = (1:N)/N; fs = N; $f = (1:N)^{s}/N;$ % Generate time vector 1 sec long % Assumed sample frequency for 1 sec data % Generate frequency vector for plotting x = t% Generate time vector x(129:N) = 0; % Generate data signal Xf = fft(x)% Take Fourier Transform, scale Mag = abs(Xf(2:end))/(N/2); % Phase = -angle(Xf(2:end))*(360/(2*pi)); % and remove first point (DC value)

plot(f(1:20),Mag(1:20),'xb'); hold on; % Plot magnitude lower frequencies) xlabel('Frequency (Hz)'); ylabel('|X(f)|'); 41





Example	3-6 ~ Re	sults (co	ontinued)			
The nume	rical value	s produc	ed by this	program	are given below.	
a _n	b _n	Cn	Mag(fft)	Theta	Phase (fft)	
-0.1033	0.1591	0.1897	0.1897	-57.0182	121.5756	
0.0020	-0.0796	0.0796	0.0796	-88.5938	-91.4063	
-0.0132	0.0530	0.0546	0.0546	-76.0053	99.7760	
0.0020	-0.0398	0.0398	0.0398	-87.1875	-92.8125	
Both met however, because th quadrant.	hods prod the angle he MATLA	uce ident s calculat .B 'atan' f	ical magn ed using unction de	itude spe direct imp bes not de	ctra; lementation are incorrect termine the correct	
 Both mag the values 	gnitudes a determin	nd the pl ed analyt	nase foun ically in E	d by the ff xample 3-	t routine match fairly closely 1.	
•Note that errors. (Ar	the value example	s for a ₂ a where ha	nd a ₄ are and calcul	not exactl ation is m	y zero due to computational ore accurate than the	44

Example 3-7 Construct a waveform consisting of a single sine wave and white noise with an SNR of -14 db. Calculate the Fourier Transform of this waveform and plot the magnitude spectrum.

<u>Solution:</u> Use sig_noise to generate the waveform, take the Fourier Transform using fft, obtain the magnitude using abs, and plot.

The routine 'sig_noise' generates data consisting of sinusoids and noise, and can be useful in evaluating spectral analysis algorithms. The calling structure for sig_noise is:

[x,t] = sig_noise([f],[SNR],N); % Generate a signal in noise

where f specifies the frequency of the sinusoid(s) in Hz, SNR specifies the desired noise associated with the sinusoid(s) in db, and N is the number of points.

If f is a vector, than a number of sinusoids are generated, each with a Signal-to-Noise ratio specified by SNR assuming it is a vector. If SNR is a scalor, its value is used for the SNR of all the frequencies generated. 45











Analysis:

To convert the heart rate data to a sequence of evenly spaced points in time, a time vector, xi, is first created that increases in increments of 1.0 second between the lowest and highest values of time in the original data.

A 1.0-second increment was chosen since this was approximately the average time spacing of the regional data.

Evenly spaced time data, yi, were generated using the MATLAB interpolation routine interp1.

This routine takes the old x and y points and the desired new x points as inputs and produces an interpolated output with the desired x point spacing.

Since the spectrum of heart rate variability is desired, the average heart rate is subtracted before evaluating the Power Spectrum.

Example 3-9 Determine and plot the frequency characteristics of heart rate variability during both normal and meditative states using

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averaging.	-			
Solution: Write a general program called welch Spectrum given the data, segment si overlapping points in adjacent segme This routine should also take in, as a sampling frequency to be used in ger Output the power spectrum and the f Output only the non-redundant points	to generate an average Power ze, and the number of nits. n optional parameter, the nerating a frequency vector. requency vector. s; i.e., up to fs/2.			
data loading and reorganizing as in %	n Example 3-8			
<pre>segment_length = fix(length(yi)/8); % Average 8 segments [PS_avg,f] = welch(yi,segment_length,segment_length-1,fs); subplot(1,2,1)</pre>				
plot(f PS_avg 'k'):	% Plot averaged PS			

plot(f,PS_avg,k'); % Plot averaged PS xlabel(Frequency (Hz)'); ylabel('Powr Spectrum'); axis([0.2 0 max(PS_avg)*1.2)); % Limit horizontal axis Repeat for meditative data 52

% O	utput argum	nents			
%	sp	spectrogram			
%	f	frequency vector for plotting			
% In	out argume	nts			
%	x data				
%	nfft wind	nfft window size			
%	noverla	noverlap number of overlaping points in adjacent segments			
%	fs sample frequency				
[N xc	ol] = size(x)	;	%		
Make	row vector				
if N <	xcol				
x =	x';				
N =	xcol;				
end					
half_s	segment = f	ix(nfft/2);	% Half segment length		
if iser	npty(noverla	ap) == 1			
noverlap = half_segment;		f_segment;	% Set default overlap at 50%		
end					
incre	ment = nfft -	noverlap;			
	$a = fi \sqrt{N}$	nfft)/incromont)	% Determine the number of segments		
nu_a	$y_{3} = iix((in)$	-min/morement/	78 Determine the number of segments		

Function 'welch' (continued)	
if isempty(fs) == 0 f = (1:half_segment)* fs/nfft:	% Calculate frequency vector
else	/·····/···//···//
f = (1:half_segment)* pi/nfft:	% Default frequency vector
end	,,,,,,,,
%	
for i = 1:nu_avgs	% Calculate spectra each segment
data = x(first_point:first_point+n	% Set up to isolate appropriate ifft-1); % data segment
if i == 1	
PS = abs((fft(data)).^2)/(nfft*nu_av else	rgs); % Calculate first PS
PS = PS + abs((fft(data)).^2)/(nfft* end	nu_avgs); % Calculate PS avg
end	
PS = PS(1:halt_segment);	% Remove redundant points
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Analysis:

The routine 'welch' illustrates a number of MATLAB tricks.

• The initial section tests the dimensions of the input to determine if it is arranged as a row or column vector. If it is a column vector, the number of rows, N, will be less than the number of columns, xcol, and the vector is transposed insuring that x in now a row vector.

• The program checks if a desired overlap is specified (i.e, noverlap is not an empty variable) and, if not, sets the overlap to a default value of 50% (i.e., half the segment length, nfft).

•A frequency vector, f, is generated from 1 to $\boldsymbol{\pi}$ if fs is unspecified, or from 1 to fs if it is given.

• The number of segments to be averaged is determined based on the segment size (nfft) and the overlap (noverlap).

• A loop is used to take the Fourier Transform of each segment, calculate the Power Spectrum, and sum the individual spectra.

•Finally the averaged Power Spectrum is shortened to eliminate 55 redundant points







